Composites by Rapid Prototyping Technology

S. Kumar, ^{a,1} J.-P. Kruth ^b

^a CSIR National Laser Centre, Pretoria, South Africa ^b Division PMA, Dept. of Mechanical Engineering, Katholieke Universiteit Leuven, Belgium

Abstract

The use of rapid prototyping (RP) technology for rapid tooling and rapid manufacturing has given rise to the development of application-oriented composites. The present paper furnishes succinct notes of the composites formed using main rapid prototyping processes such as Selective Laser Sintering/Melting, Laser Engineered Net Shaping, Laminated Object Manufacturing, Stereolithography, Fused Deposition Modeling, Three Dimensional Printing and Ultrasonic Consolidation. The emphasis of the present work is on the methodology of composite formation and the reporting of various materials used.

Key words: : Rapid Prototyping (RP), Laser, Composites

1 Introduction

Rapid Prototyping (RP) initially focussed on polymers. These were later replaced/supplemented by ceramics, metals and composites. Composites are used in RP not only to make desired product but also to facilitate the process. For example in Fused Deposition Modeling (FDM), a blend of various polymers may be used, in which different polymers play the role of tackifier, plasticizer, surfactant etc.

There are a number of RP techniques in vogue but only some of them have been used for the production of composites. The processes which have mainly been employed for fabricating composites are: Selective Laser Sintering/Melting

¹ corresponding author. Address: Dr. Sanjay Kumar, CSIR National Laser Centre, PO Box 395, Pretoria 0001, South Africa, Tel: +27128414138, Fax: +27128413008, Email: skumar@csir.co.za

(SLS/SLM), Laser Engineered Net Shaping (LENS), Laminated Object Manufacturing (LOM), stereolithography (SL), Fused Deposition Modeling (FDM), Three Dimensional Printing (3DP) and Ultrasonic Consolidation (UC) [1–3]. The present paper deals with only the above mentioned RP techniques.

Fibre-reinforced composites have been produced by some of the RP techniques and the paper deals with them. RP techniques which have been mainly used with fibre-based composites are SL, FDM and LOM. In a powder-based RP technique such as SLS [4] and LENS, it is difficult to draw smooth layers of powder-fibre mixture [5]. Using long or continuous fibres instead of short fibres is difficult to incorporate into processing and its use has been limited solely to LOM and SL techniques [6,7]. In FDM and LOM, fabrication of respective fibre-reinforced composite filaments tapes and laminates are required as a pre-step before RP processing, necessitating the need for materials to be formulated and developed.

RP techniques are increasingly used for making biocomposites and a section is devoted to it. Not much work has been done in the area of nanocomposite, the paper nevertheless devotes a short section to it.

2 Selective Laser Sintering/Melting (SLS/SLM)

There are two main reasons for processing composites by SLS/SLM [4]: 1) to facilitate the SLS process using liquid phase sintering (LPS) mechanism and, 2) to combine various materials for achieving properties unachievable by a single material. Examples of first type are the SLS of Fe-Cu, where Cu acts as a melted fluid during processing and binds Fe powders to help form a composite of Fe-Cu [8]. In this case, Cu is not added to enhance the mechanical or other properties of iron product but only to help consolidate the iron powders without difficulty.

The second type is the emulation of formation of traditional composites using SLS/SLM processes, e.g. SLS of PCL/HA, where hydroxypatite (HA) is added to polycapralactone (PCL) for enhancing its strength and biocompatibility [9]. The present section deals only with manufacturing of this type of composites.

In SLS/SLM, composites have been manufactured mainly by using three methods which have been elaborated in the coming subsections.

This is the most common method used for consolidating a composite. Most noticeable application is the formation of a Polymer Matrix Composites (PMC) and the binding mechanism involved is Liquid Phase Sintering (LPS). Polymer powders and ceramics are mixed and laser sintered to form the composites, e.g. PCL and HA [9], Polyether ether ketone (PEEK) and HA [10], PE and HA [11], PA and nano-clay [5] etc. It has been found that Polymethyl mathacrelate (PMMA)-coated HA powder could facilitate better binding of the composite, but uncoated powder is used for the reason of biocompatibility. Coating of a powder has certain other advantages. In case of a nano Al₂O₃ and PS composite, nano Al₂O₃ particles are coated with PS to prevent the agglomeration of nano particles resulting in a uniform distribution of particles in the polymer matrix [12].

The reinforcement powder is used in the form of particulates because fibres as a reinforcement give problems during formation of a smooth powder bed and are not helpful in increasing the final density and strength. Instead of taking a mixture of a polymer powder and a reinforcement powder, a single composite powder can also be used, e.g. glass-filled polyamide (PA) powder, Al-filled PA powder [13,14], HA-filled HDPE powder [15], TCP-glass powder [16] etc. A single composite particle helps overcome the difficulty associated with mixing the powders and yields a uniform spread of composite components in the final product. However, if one of the component of the composite powder is a fiber, problems of manufacturing occur.

The method has also been used to make Metal Matrix Composite (MMC), e.g. Fe and graphite [17], WC-Co [18,19], WC-Co and Cu [20,21], Fe, Ni and TiC [22] etc and Ceramic Matrix Composite (CMC) e.g. SiSic [23]. SLS of ceramic and metal, in general, does not give as dense products as is found in the case of PMC. In order to fully consolidate it, an extra material is added to the powder mixture [21] or the porous product is infiltrated [18,19]. Addition of La₂O₃ to the mixture of WC-Co and Cu decreases the surface tension of the melt and consequently increases its sinterability [21]. Strengthening of a WC and Co green product may be done by infiltrating it with bronze [18,19,24,25]. An image of a bronze (Cu and 10% Sn) infiltrated WC-12Co by BSE (Backscattered Electron) mode of SEM is shown in Figure 1 [25].

Table 1 summarizes various materials used for direct fabrication of composites in SLS.

Various customized composite powders are available for processing such as DuraForm GF (polyamide and glass fibre), DuraForm AF (polyamide and aluminium) [34]. A polyamide powder with short carbon fibre reinforcement

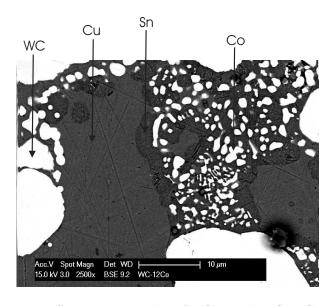


Fig. 1. SEM micrographs of infiltrated WC-12Co

is also available [4].

2.2 Manufacturing of Composites using In-situ Reactions

Laser-induced chemical reactions are used to create in-situ particles during laser sintering. The energy of the laser beam can be used in two ways: 1) to overcome the activation energy of the reactants and to form chemical compounds and 2) to trigger a chemical reaction which will not only form a compound but generate enough thermal energy to propagate chemical reactions. Both types of in-situ formation of compounds are better than the pre-addition of compounds because of the following reasons: fine and uniform distribution of compounds, better wetting, release of exothermic energy helpful to binding.

Examples of 1st type are the formation of Cu-based MMC reinforced with TiB₂ and TiC from a powder mixture of Cu, Ti and B₄C [35]. The 2nd type is a case of Self-propagating High-temperature Synthesis (SHS), e.g. formation of TiC- Al₂O₃ composite from TiO₂, Al and C [28]; Al₂O₃-Cu composite from CuO and Al [36]; NiTi-HA composite from Ni, Ti and HA [37,38]. In the latter case, it has been found that though the product is porous, it could be suitable as an implant material.

Chemical reactions may also help creating a binder material in the case of laser processing of SiC, where disintegration of SiC and subsequent reaction with O₂ gas forms SiO₂ which binds rest SiC powders [39]. This manufacturing mechanism has not furnished strong parts and has not been further used.

Post-processing of laser sintered materials in a furnace is another way for manufacturing a composite. It has been mainly performed in two ways: 1) by using the furnace for infiltration with or without preceding debinding, 2) by using the furnace for chemical reaction and infiltration.

Examples of the first type are treating laser sintered acrylic/glass product in a furnace where the acrylic binder gets de-binded and the glass (SiO₂-Al₂O₃-P₂O₅-CaO-CaF₂) partially changes to ceramic (with apatite and mullite phase) making a glass-ceramic composite [40,41]. In this case, the composite was manufactured using a furnace cycle without using infiltration. In another case, a laser sintered polymer-coated SiC powder was infiltrated with Al in a furnace to form MMC [42]. Other examples are: the formation of refractory Mo-Cu composite [43], silver infiltration of a high-temperature superconducting ceramic Y₂BaCu₃O_{7-x} [44], aluminium infiltration of Al₂O₃ and SiC [45]

The 2nd type is most common and the most used example is the formation of Si/SiC composites. Laser processed SiC is treated with a phenolic resin. The resin after curing in a furnace gives rise to carbon which reacts with some of the infiltrant Si to form SiC and produces finally Si-SiC composite. The amount of SiC in the composite could be controlled by the degree of treatment of the green product with phenolic resin [46–48]. Another noticeable example of chemical reaction inside a furnace is the use of nitrogen gas for reacting with green product of Al alloy to form AlN. Its infiltration with Al alloy later, produces Al MMC. In this case, successfully manufacturing of Al composite is dependent upon the strength furnished to the meso structure by the formation of nitride [49,50].

3 Three Dimensional Printing (3DP)

Three Dimensional Printing (3DP) is a powder-based RP process in which a polymer binder is jetted onto pre-deposited powder layers. Composites could be made by changing a component of the powder mixture, provided they are compatible with the jetted polymer binder. Here, compatible means that the powders should not be dissolved or chemically react in presence of the polymer.

3DP gives a unique opportunity to control the material composition [51,52] of the product by jetting different materials from different nozzles. These jetting materials can be used either in a molten form or in a slurry form. This can help manipulate various properties such as electrical conductivity, thermal

conductivity, reflectivity, magnetic properties and hardness at various places of the product and make Functionally Graded Materials (FGM) or composites [53,54].

Infiltrating porous preform of ceramics, obtained by 3DP with metal or alloy is again an option common to all RP techniques for making composites [55]. A part containing 60 % stainless steel and 40% copper or starch + polyurethane or starch + surgical wax has been successfully made [53].

It is difficult to make fiber-reinforced composite either by jetting the fiber or using a powder-fiber mixture. Infiltration with fiber could help make composite. There is evidence that carbon nano fiber could be infiltrated along with polymer (epoxy resisn) to enhance electrical conductivity [56].

Table 2 summarizes main materials used for fabrication of composites in 3DP.

4 Laser Engineered Net Shaping (LENS)

Laser Engineered Net Shaping (LENS) is similar to SLS as it is also a powderand laser-based technique; the main difference between the two processes is the way the powder is deposited. The fabrication of composite in LENS is similar to SLS with regard to laser-powder interaction [58–60]. In one variant of LENS named CMB [61], there is an option to use a wire instead of powder as a starting building material [62] giving possibility to make composites without using powders unlike SLS.

LENS is used to create composites having varying degrees of reinforcement composition leading to Functionally Graded Materials (FGM) by using different powders carried using non-reactive gases from different nozzles [58].

Table 3 summarizes various materials used for the direct fabrication of composites in LENS.

5 Laminated Object Manufacturing (LOM)

Fabrication of composites by LOM directly depends upon development of composite laminates. Particulate or fibre reinforced sheets are needed to be produced in order to be further processed for fabricating composites. Fabrication could also be accomplished by infiltrating a preform after a binder burn-out cycle. Pressure is applied during the binder burn-out cycle for avoiding any possible delamination. This could be executed by applying an uniaxial

press to an enclosed chamber housing LOM parts covered in silica powders. The powder helps the pressure to be distributed evenly and release degraded binder [68,6].

LOM is unique in the sense that layers of the product could be changed with laminates made up of different materials composition to make varied composites. It has been used to develop a FGM or composite of TiC/Ni with the help of combustion synthesis as post-processing [69]. This possibility has its limitation for automating, as many different sets of laminates need to be integrated into the process.

Fiber-reinforced Composite in LOM

In LOM, there is an example of making a FRC sheet of 0.5 mm by joining layers of ceramic tapes with fibre prepegs. Fibre prepegs are fabricated by joining an unidirectional continuous fibre with a thermosetting resin. During LOM processing, cutting of the continuous ceramic fibres with the CO₂ laser produces burning and heat damage to the adjacent polymer. This problem could be avoided by using copper vapour lasers as it cuts the fibre by photoablation mechanism [68]. In another case, a LOM product is developed from binding a pyrolysed filter paper made up of cellulose fibres with an adhesive tape developed from a slurry containing phenolic resin, polyvinyl butyral, benzyl butyl phthalate and ethanol. The product is then again pyrolysed at 800°C in nitrogen atmosphere to convert the phenolic resin into carbon. The porous carbonized samples were then post-infiltrated with liquid Si in vacuum at 1500°C for making FRC [70].

6 Stereo-Lithography (SL)

In order to fabricate composite by SL, a photopolymer is mixed with particulates or fibres which furnishes enhanced properties. Reinforcing particles give rise to an increase in the viscosity of the photopolymer which consequently complicates the coating process of new layers. Other problems associated with a liquid mixture are: 1) particulate getting settled instead of being suspended in the liquid resin resulting in a non-uniform distribution of reinforcing particles, 2) formation of bubbles in the liquid giving rise to pores after curing which become sources of potential crack initiation, 3) requirement of longer duration of curing due to lower absorption of laser energy by the liquid, arising out of partial reflection of laser rays by the solid particles present in the liquid [7,71,72]. Some of the aforementioned problems can be avoided by using a variant of SL, i.e. the Optoform process in which a paste containing various materials replaces the photopolymer liquid [73].

Using thermal curing in addition to photo-curing also helps make composites by strengthening specially developed polymer mixtures [74].

Fiber-reinforced Composite in SL

Out of all techniques, SL is the one which has been mostly employed for investigating FRC using short fibres [75], continuous fibres [76] and fibre mats [7]. Selection of a glass fibre instead of a ceramic or carbon one decreases its opacity to UV light [77] which makes glass fibre more SL-friendly for making FRC.

Though, continuous fibre is ideal for enhancing mechanical properties, mixtures with short fibres of higher aspect ratio shows more or less comparable properties [77]. Increasing the volume fraction augment the properties but is restrained by the increasing difficulty in the layer formation and the post-processing. However, surface coating of the fibre helps decreasing the viscosity of the mixture [78]. Fibres also support inter-layer bonding by getting partially settled into the uncured regions of a previous layer [75]. The efficiency of short fibres is constrained by their non-uniform distribution in length, random orientation in mixture and fracture during mixing [77].

Table 4 summarizes materials used for fabricating FRC in SL.

7 Fused Deposition Modeling (FDM)

Fused Deposition Modeling (FDM) is capable of yielding strong composite parts as bond forms between successive roads and layers due to partial or full melting of the feedstock composite filaments. In the case an overhanging section is to be produced, a removable support structure of wax has to be created using another nozzle.

Feedstock development is essential for manufacturing a composite product by FDM. The feedstock filament must be of right composition and strength and must furnish a low-viscous extruded material. It consists of a base polymer, a tackifier, a plasticizer and a surfactant besides other metals, polymers or/and ceramics. The base polymer gives strength so that the filament acts as a piston during processing. The tackifier is used for tackiness and flexibility, the plasticizer for improving the flow and the surfactant for an enhanced homogeneous dispersion of metal/ceramic in solution. The development of the filament needs the mixing of right amounts of these components [79,80].

Table 5 summarizes main materials used for the fabrication of composites in FDM.

Fiber-reinforced Composite in FDM

Addition of fibres in case of FDM increases the stiffness of the thermoplastic and decreases the swelling of the tape at the extrusion die head during its production [83]. It also increases its brittleness making it difficult to get wound on a cylindrical drum for getting further operated. Its ductility and flexibility can be improved by the addition of a linear polymer into the mixture. Presence of fibre also enhances the softening temperature and the heat distortion temperature of tapes [84]. Fibres of higher aspect ratio (L/D>100) can be generated during extrusion of tapes by an introduction of droplets of Thermotropic Liquid Crystalline Polymers (TLCP) into the mixture. TLCP can also help overcome problems of extruding fibres of higher aspect ratio through the small diameter FDM die head as they are susceptible to fracture during extrusion. The morphology of TLCP reinforced polymer depends on shear and extensional flow fields during processing and can be tailored to give the required properties. As the processing temperature of TLCP is high and, gives rise to degradation of the base thermoplastic during melting of the mixture, it is necessary to melt them separately and then blend later [85].

8 Ultrasonic Consolidation (UC)

UC is mainly a metallic foil based technique and is suitable for the formation of metal composite structures or metal-matrix composite. The foils are bonded by ultrasonic welding and the bonding parameters are limited by few types of existing UC machines. The foils used are mainly Al, Cu, Fe, Ni etc [86–89].

The process gives following advantages over other RP techniques for making FRC:

- (1) Precise placement of fiber in the structure,
- (2) Lack of damage of sensitive fibre because of low rise of temperature,

SiC fiber and shape memory alloy fiber have been yet successfully bonded [90,91]. A commercial composite foil named MetPreg (alumina fiber embedded over Al foil) has also been used to observe its bondability [92].

9 Fabrication of Nanocomposites

Polymer matrix nanocomposite have already been made by RP techniques while little work has been done for utilizing nano particles in fabricating metal matrix composites.

There are inherent limitations in using nano particles in powder-based RP techniques such as SLS, LENS and 3DP because it will decrease the tap density and processability. However, nano-structured powder of micron size can be used for nano effect [5,93,67]. Presence of nano-particles into polymer inhibits movement of polymer macromolecules and increases tensile modulus and strength of the polymer without reducing its impact resistance. However, a higher volume fraction is unsuitable as it decreases final green density [5].

In SL and FDM, by using small volume fractions of nano-additives, thermal [83], optical [94] and mechanical properties [95,96] of a matrix polymer can be enhanced without increasing viscosity of the mixture. It eliminates difficulties associated with processing high-viscous materials in SL and FDM. It is also possible to increase the volume fractions by more than 40% [97].

Addition of nano-particles in a resin for SL helps them to get evenly dispersed without constantly agitating the mixture. A material, Bluestone containing nano-ceramic has been developed for SL which makes parts suitable for electrical housing [98].

10 Composites for Bio-medical Applications

Besides the use of RP techniques to produce scaffolds of plain Ti alloys [99–101] or plain biocompatible polymers [102–104], RP has also been used for manufacturing scaffolds [62,105,10,106–109] and custom medical implants [110,111] out of polymer-ceramic composites. These biocompatible composites can be bioactive, bioinert or of various degrees of bio-resorbability. Biodegradable composites are of new interest as implant materials in tissue engineering because: 1) it eliminates the need for a second surgical operation, done for removing implants after healing, and 2) it gives less possibility of a mismatch of the mechanical properties between bones and implants [112,113].

RP has the following special advantages over the conventional techniques for fabricating scaffolds and this explains its increasing acceptability: freedom of shape and size, controlled creation and distribution of global pores of various sizes and shapes, free from toxic binders and solvents and, the capacity for precision and reproducibility. RP has also been combined with conventional techniques to take advantages of both, for the creation of scaffolds. RP has created designed global pores while conventional techniques make local pores necessary for providing potential space for tissue growth. Global pores serve the purpose of nutrient diffusion, fluid and blood flow, control of cell growth and tissue differentiation [107].

The addition of Ca-P ceramic to the polymer makes a composite bone analogue

and improves the bone bonding behaviour of unfilled polymers [113]. Calcium phosphate increases the osteoconductivity of the biocomposite [124]. It has been found that the right amount of HA is required to enhance the bioactivity of polymers without making the composites fragile. In case of a PEEK/HA mixture, the right amount of HA is about 40% [10].

Bioactive glasses and glass ceramics are other notable fillers besides HA to polymers [113]. The biocomposite of Titanium nickelide (NiTi) and HA has been synthesized for fabricating bone implants from a mixture of Ni-Ti powder and HA additive through SHS mechanism by the SLS technique [37]. LOM has also been employed to manufacture a custom bone implants from a sheet of $125-150\mu$ m consisting of calcium hydroxyapatite and calcium phosphate glass. Pore sizes of post-processed LOM implants depend upon the size of HA and can be enlarged by taking large particles [111]. Table 6 shows the materials used by various RP techniques for fabricating bio-composites.

11 Conclusion

Composites have been fabricated using RP techniques mainly for mechanical applications while its utility for other inter-disciplinary applications namely, optical, electronic and thermal, barring few exceptions, has not yet been extensively investigated. There is need to develop either existing RP techniques (such as increasing the capacity of UC/SLM machine etc.) or search for a new RP technique (such as based on plasma welding etc.) in order to enhance the application domain.

SL and LOM have vast potentials for the fabrication of continuous fiber reinforced composites. However for fast and accurate reproducibility, the techniques need to be further matured. SLS and LENS are capable of producing in-situ ceramics for formation of composites and offers a distinguished area for further exploration. The development of special powders is the easiest way to make composites using SLS/LENS/3DP.

Production of bio-composite specially for manufacturing of scaffolds is another field in which RP has distinct advantages over conventional techniques and with present pace of development, will get more attention in future.

References

[1] Levy G, Schindel R, and Kruth JP. Rapid manufacturing and rapid tooling with layer manufacturing technologies: State of the art and future perspectives.

- Ann CIRP 2003; 52(2): 589-609.
- [2] Pham DT, Dimov SS, Ji C, and Gault RS. Layer manufacturing processes: Technology advances and research challenges. Pro VRAP 2003, Portugal: 107-113.
- [3] Kumar S. SLS of Iron-based Powders and SLS/SLM for Rapid Tooling. PhD thesis 2008; K. U. Leuven, Belgium.
- [4] Kruth JP, Levy G, Klocke F, and Childs T. Consolidation phenomena in laser and powder-bed based layer manufacturing. Ann CIRP 2007; 56(2): 730-59.
- [5] Kim J and Creasy TS. Selective laser sintering characteristics of nylon 6/clayreinforced nanocomposite. Poly Test 2004; 23:629-36.
- [6] Klosterman D, Chartoff R, Graves G, Osborne N, and Priore B. Interfacial characteristics of composites fabricated by laminated object manufacturing. Compo Part A 1998; 29A: 1165-74.
- [7] Karalekas DE. Study of the mechanical properties of nonwoven fibre mat reinforced photopolymers used in rapid prototyping. Mat & Des 2003; 24:665-70.
- [8] Kruth JP, Van der Scheuren B, Bonse JE, and Morren B. Basic powder metallurgical aspects in selective metal powder sintering. Ann CIRP 1996; 45(1):183-86.
- [9] Wiria FE, Leong KF, Chua CK, and Liu Y. Poly-e-capralactone/hydroxyapatite for tissue engineering scaffold fabrication by selective laser sintering. Acta Biomat 2007; 3(1): 1-12.
- [10] Tan KH, Chua CK, Leong KF, Cheah CM, Cheang P, Abu Bakar MS, et al. Scaffold development using selective laser sintering of polyetheretherketone-hydroxyapatite biocomposite blends. Biomat 2003;24:3115-23.
- [11] Hao L, Savalani MM, Zhang Y, et.al. Effect of material morphology and processing conditions on the characteristics of hydroxyapatite and high-density polyethylene biocomposite by selective laser sintering. Pro inst mech engineers Part L: J Mat Des and App 2006; 220(L3):125-37.
- [12] Zheng H, Zhang J, Lu S, Wang G, and Xu Z. Effect of core-shell composite particles on the sintering behaviour and properties of nano- Al_2O_3 /Polysterene composites prepared by SLS. Mat Let 2006; 60 (9-10): 1219-23.
- [13] Mazzoli A, Moriconi G, and Pauri MG. Characterization of an aluminium-filled polyamide powder for applications in selective laser sintering. Mat & Des 2007; 28 (3): 993-1000.
- [14] Beer DJD and Booysen GJ. Rapid tooling using Alumide. Pro VRAP 2005;387-94.
- [15] Savalani MM, Hao L, and Harris RA. Evaluation of CO_2 and Nd:YAG lasers for the selective laser sintering of HAPEX(R). Pro Inst Mech Eng Part B J Eng Manu 2006; 220 (2):171-182.

- [16] Wilkes J and Wissenbach K. Rapid manufacturing of ceramic components for medical and technical applications via selective laser melting. Pro Euro-uRapid 2006; Frankfurt, A4/1.
- [17] Simchi A and Pohl H. Direct laser sintering of iron-graphite powder mixture. Mat Sc & Eng A 2004; 383 (2): 191-200.
- [18] Laoui T, Froyen L, and Kruth JP. Effect of mechanical alloying on selective laser sintering of WC-9CO powder. Powder Metal 2000; 42 (3):203-205.
- [19] Maeda K and Childs THC. Laser sintering (SLS) of hard metal powders for abrasion resistant coatings. J Mater Pro Techno 2004; 149(1-3):609-15.
- [20] Gu D and Shen Y. WC-Co particulate reinforcing Cu matrix composites produced by direct laser sintering. Mater Let 2006; 60 (29-30): 3664-3668.
- [21] Gu D, Shen Y, Zhao L, Xiao J, Wu P, and Zhu Y. Effect of rare earth oxide addition on microstructures of ultra-fine WC-Co particulate reinforced Cu matrix composites prepared by direct laser sintering. Mat Sci and Eng A 2007; 445-446: 316-322.
- [22] Gaard A, Krakhmalev P, and Bergstrom J. Microstructural characterization and wear behaviour of (Fe,Ni)-TiC MMC prepared by DMLS . J Alloys and Comp 2006; 421 (1-2): 166-71.
- [23] Exner H, Horn M, Streek A, Regenfuss P, Ullmann F, and Ebert R. Laser micro sintering- a new method to generate metal and ceramic parts of high resolution with sub-micrometer powder. Pro VRAP 2007; Portugal: 491-9.
- [24] Kumar S, Kruth JP, and Froyen L. Wear Behaviour of SLS WC-Co Composites. Pro SFF 2008; Texas: 543-57.
- [25] Kumar S. Manufacturing of WC-Co Moulds using SLS Machine. J Mat Pro Techno 2009; 209: 3840- 48.
- [26] Vaucher S, Paraschivescu D, Andre C, and Beffort O. Selective laser sintering of aluminium-silicon carbide metal matrix composites. Mater Week 2002.
- [27] Lu L, Fu JYH, Chen ZD, Leong CC, and Wong YS. In-situ formation of TiC composite using selective laser melting. Mat Res Bulletin 2000; 35:1555- 61.
- [28] Slocombe A and Li L. Selective laser sintering of TiC-Al₂O₃ composite with self-propagating high-temperature synthesis. J Mat Pro Techno 2001; 118: 173-8.
- [29] Hon KKB and Gill TJ. Selective laser sintering of SiC/Polyamide composites. Ann CIRP 2003; 52(1): 173- 6.
- [30] Ho HCH, Cheung WL, and Gibson I. Effects of graphite powder on the laser sintering behaviour of polycarbonate. Rapid Proto J 2002; 8 (4):233-42.
- [31] Ramesh CS, Srinivas CK, and Channabasappa BH. Abrasive wear behaviour of laser-sintered iron-SiC composites. Wear 2009; DOI 10.1016/j.wear2008.12.026.

- [32] Shishkovsky I, Yadroitsev I, Bertrand P, and Smurov I. Alumina-zirconium ceramic synthesis by selective laser sintering/melting. App Surf Sci 2007; 254: 966-70.
- [33] Fan KM, Cheung WL, and Gibson I. Fusion behaviour of TrueForm (TM)/SiO₂ composite powders during selective laser sintering. Rapid Proto J 2008; 14 (2):87-94.
- [34] 3D Systems. http://www.3dsystems.com.
- [35] Leong CC, Lu L, Fu JYH, and Wong YS. In-situ formation of copper matrix composites by laser sintering. Mat Sci and Eng A 2002; 338:81-8.
- [36] Kamitani T, Yamada O, and Marutani Y. Selective laser sintering with heat of formation by using reactive materials. Pro SPIE 2000; 4088:299-302.
- [37] Shishkovskii IV, Tarasov EY, Zhuravel LV, and Petrov AL. Selective laser sintering in the powder synthesis of a biocomposite based on titanium nickelide and hydroxyapatite. Tech Phy Let 2001; 27 (3):211-3.
- [38] Shishkovsky IV, Tarasova E, and Petrov A. Synthesis of biocomposite on the base of niti with hydroxyapatite by selective laser sintering. Pro LANE 2001;459-64.
- [39] Klocke F and Wirtz H. Selective laser sintering of ceramics. Pro LANE 1997; 589-596.
- [40] Goodridge RD, Wood DJ, Ohtsuki C, and Dalgarno KW. Biological evaluation of an apatite-mullite glass-ceramic produced via selective laser sintering. Acta Biomater 2007; 3(2):221-31.
- [41] Dalgarno KW, Wood DJ, et.al. Mechanical properties and biological responses of bioactive glass ceramic processed using indirect SLS. Pro SFF 2005; Texas: 132-40.
- [42] Alexandre T, Giovanola J, Vaucher S, Beffort O, and Vogt U. Layered manufacturing of porous ceramic parts from ceramic powders and preceramic polymers. Pro LANE 2004;Germany: 497-504.
- [43] Liu B, Bai PK, and Cheng J. Microstructure evolution of Mo-based composites during selective laser sintering and thermal processing. J Compu and Theo Nanosci 2008;5(8):1565-69.
- [44] Agarwala MK, Bourell DL, Manthiram A, Birmingham BR, and Marcus HL. Synthesis, Selective laser sintering and infiltration of High T_c dual phase $Y_2BaCu_3O_{7-x}$ supercondutor composites. Pro SFF 1993; Texas: 339-49.
- [45] Deckard L and Dennis Claar T. Fabrication of ceramic and metal matrix composites from selective laser sintered preforms. Pro SFF 1993; Texas:215-22.
- [46] Lenk R, Nagy A, and Techel A. Material development for laser sintering of high temperature strength silicon carbide with extern hardness. Pro Euro-uRapid 2003; Frankfurt: B/4.

- [47] Evans RS, Bourell DL, Beaman JJ, and Campbell MI. Rapid manufacturing of silicon carbide composites. Rapid Proto J 2005; 11 (1): 37-40.
- [48] Stevinson BY, Bourell DL, and Beaman JJ. Over-infiltration mechanisms in selective laser sintered Si/Sic preforms. Rapid Proto J 2008; 14 (3):149-54.
- [49] Sercombe TB and Schaffer GB. On the role of magnesium and nitrogen in the infiltration of aluminium by aluminium for rapid prototyping applications. Acta Mater 2004; 52(10):3019-25.
- [50] Yu P and Schaffer GB. Microstructural evolution during pressureless infiltration of aluminium alloy parts fabricated by selective laser sintering. Acta Mater 2009; 57: 163-70.
- [51] Jackson TR, Liu H, Patrikalakis NM, Sachs EM, and Kima MJ. Modeling and designing functionally graded material components for fabrication with local composition control. Mat & Des 1999; 20 (2-3):63-75.
- [52] Cho W, Sachs EM, Patrikalakis NM, and Troxel DE. A dithering algorithm for local composition control with three-dimensional printing. Computer-Aided Design 2003; 355 (9): 851-67.
- [53] Dimitrov D, Schreve K, and De Beer N. Advances in three dimensional printing- state of the art and future perspectives. Rapid Proto J 2006; 12 (3): 136-47.
- [54] Kernan BD and Sachs EM. Three dimensional printing of tungsten carbide-cobalt using a cobalt oxide precursor. Pro SFF 2003; Texas: 616-31.
- [55] Rambo CR, Travitzky N, Zimmermann K, and Greil P. Synthesis of TiC/Ti-Cu composites by pressureless reactive infiltration of TiCu alloy into carbon preforms fabricated by 3D-printing. Mat Let 2005; 59: 1028-31.
- [56] Czyzewski J, Burzynski P, Gawel K, and Meisner J. Rapid Prototyping of electrically conductive components using 3D printing technology. J Mat Pro Techno 2009; 209 (12-13): 5281- 5.
- [57] http://www.prometal.com.
- [58] Liu W and Dupont JN. Fabrication of functionally graded TiC/Ti composites by Laser Engineered Net Shaping. Scripta Mater 2003; 48: 1337-1342.
- [59] Banerjee R, Collins RC, Genc A, and Fraser HL. Direct laser deposition of in situ Ti-6Al-4V-TiB composites. Mat Sci and Eng A 2003; 358: 343-9.
- [60] Li XC, Stampfl J, and Prinz FB. Mechanical and thermal expansion behaviour of laser deposited metal matrix composites of Invar and TiC. Mat Sci and Eng A 2000; 282: 86-90.
- [61] Klocke F and Freyer C. Quick manufacture, repair and modification of steel moulds suing controlled metal build up (CMB). Pro LANE 2004; Germany: 579-587.

- [62] Beaman JJ, Antwood C, Bergman TL, Bourell D, Hollister S, and Rosen D. WTEC panel report on additive/subtractive manufacturing research and development in europe. World Technology Evaluation Centre Inc., Baltimore, Maryland 21224, 2004.
- [63] Banerjee R, Genc A, Collins PC, and Fraser HL. Comparison of microstructural evolution in laser-deposited and arc-melted in-situ Ti-TiB composites. Met and Mat Trans A- Phy Metal and Mat Sci 2004; 35A (7):2143-52.
- [64] Theiler C, Seefeld T, and Sepold G. Deposition of graded metal matrix composites by laser beam cladding. Pro LANE 2001; Germany: 421-430.
- [65] Liu WP and Dupont JN. Fabrication of carbide-particle-reinforced titanium aluminide-matrix composites by laser engineered net shaping. Met and Mat Trans A- Phy Metal and Mat Sci 2004; 35A (3):1133-40.
- [66] Xiong Y, Smugeresky JE, Ajdelsztajn L, and Schoenung JM. Fabrication of wc-co cermets by laser engineered net shaping. Mat Sci and Eng A 2008; 493 (1-2): 261- 6.
- [67] Xiong Y, Smugeresky JE, and Schoenung JM. The influence of working distance on laser deposited wc-co. J Mat Pro Techno 2009; 209 (10):4935-41.
- [68] Klosterman DA, Chartoff RP, Osborne NR, Graves GA, Lightman A, Han G, et al. Development of a curved layer LOM process for monolithic ceramics and ceramic matrix composites. Rapid Proto J 1999; 5 (2):61-71.
- [69] Zhan Y, Han J, Zhang X, He X, Li Z, and Du S. Rapid prototyping and combustion synthesis of TiC/Ni functionally gradient materials. Mat Sci and Eng A 2001; 299: 218-24.
- [70] Weisensel L, Travitzky N, Sieber H, and Greil P. Laminated Object Manufacturing (LOM) of SiSiC Composites. Adv Eng Mat 2004; 6 (11): 899-903.
- [71] Karalekas D and Antoniou K. Composite rapid prototyping: overcoming the drawback of poor mechanical properties. J Mat Pro Techno 2004;153-154: 526-30.
- [72] Cheah CM, Fuh JYH, Nee AYC, and Lu L. Mechanical characteristics of fibre-filled photo-polymer used in stereolithography. Rapid Proto J 1999; 5 (3): 112-9.
- [73] Vaneetveld G, Clarinval AM, Dormal T, Noben JC, and Lecomte-Beckers J. Optimization of the formulation and post-treatment of stainless steel for rapid manufacturing. J Mat Pro Techno 2008; 196 (1-3): 160-4.
- [74] Gupta A and Ogale AA. Dual curing of carbon reinforced photoresins for rapid prototyping. Poly Composites 2004; 23 (6): 1162-70.

- [75] Zak G, Haberer M, Park CB, and Benhabib B. Mechanical properties of shortfibre layered composites: prediction and experiment. Rapid Proto J 2000; 6 (2): 107-18.
- [76] Greer C, McLaurin J, and Ogale AA. Processing of carbon fiber reinforced composites by three dimensional photolithography. Pro SFF 1996; Texas: 307-11.
- [77] Lu L, Fuh J, and Wong YS. Laser-induced materials and processes for rapid prototyping. Kluwer Academic Publishers, Massachusetts 02061, USA, 2001.
- [78] Zak G, Chan AYF, Park CB, and Benhabib B. Viscosity analysis of photopolymer and glass-fiber composites for rapid layered manufacturing. Rapid Proto J 1996; 2 (3): 16-23.
- [79] Onagoruwa S, Bose S, and Bandyopadhyay A. Fused Deposition of Ceramics (FDC) and Composites. Pro SFF 2001; Texas: 224-31.
- [80] Masood SH and Song WQ. Development of new metal/polymer materials for rapid tooling using fused deposition modeling. Mat & Des 2004; 25:587-94.
- [81] Bandyopadhyay A, Atisivan R, Kuhn G, and Yeruva S. Mechanical properties of interconnected phase alumina-Al composites. Pro SFF 2000; Texas: 24-31.
- [82] Bandyopadhyay A, Panda RK, McNulty TF, Mohammadi F, Danforth SC, and Safari A. Peizoelectric ceramics and composites via rapid prototyping techniques. Rapid Proto J 1998; 4 (1): 37-49.
- [83] Shofner ML, Lozano K, Rodriguez-Marcias FJ, and Barrera EV. Nanofiber-reinforced polymers prepared by fused deposition modeling. J App Poly Sci 2001; 89 (11): 3081-90.
- [84] Zhong W, Li F, Zhang Z, Song L, and Li Z. Short fiber reinforced composites for fused deposition modeling. Mat Sci and Eng A 2001;301: 125- 30.
- [85] GrayIV RW, Baird DG, and Bohn JH. Effects of processing conditions on short TLCP fiber reinforced FDM parts. Rapid Proto J 1998; 4 (1): 14-25.
- [86] Kong CY, Soar RC, and Dickens PM. Characterization of aluminium alloys 6061 for the ultrasonic consolidation process. Mat Sci and Eng A 2003; 363(1-2): 99-106.
- [87] Kong CY, Soar RC, and Dickens PM. Optimal process parameters for ultrasonic consolidation of 3003 aluminium. J Mat Pro Techno 2004; 146 (2): 181-7.
- [88] Kong CY and Soar RC. Fabrication of metal-matrix composites and adaptive composites using ultrasonic consolidation process. Mat Sci and Eng A 2005; 412 (1-2): 12-8.
- [89] Janaki Ram GD, Yang Y, and Stucker BE. Effect of process parameters on bond formation during ultrasonic consolidation of aluminium alloy 3003. J Manu Systems 2006; 25 (3) 221-38.

- [90] Kong CY, Soar RC, and Dickens PM. Ultrasonic consolidation for embedding SMA fibres within aluminium matrices. Comp Structures 2004; 66 (1-4): 421-7.
- [91] Yang Y, Janaki Ram GD, and Stucker BE. Bond formation and fiber embedment during ultrasonic consolidation. J Mat Pro Techno 2009; 209 (10) 4915-24.
- [92] Janaki Ram GD, Robinson C, Yang Y, and Stucker BE. Use of ultrasonic consolidation for formation of mult-material structures. Rapid Proto J 2007; 13(4): 226-35.
- [93] Chung H and Das S. Functionally graded Nylon-11/silica nanocomposites produced by selective laser sintering. Mat Sci and Eng A 2008; 487 (1-2): 251-7.
- [94] Chartoff R, McMorrow B, and Lucas P. Functionally graded polymer matrix nano-composites by solid freeform fabrication: a preliminary report. Pro SFF 2003; Texas: 385-91.
- [95] Hadipoespito GW, Yang Y, Choi H, Ning G, and Li X. Digital micromirror device based microstereolithography for micro structures of transparent photopolymer and nanocomposites. Pro SFF 2003; Texas: 13-24.
- [96] Chryssolouris G, Stavropoulos P, Tsoukantas G, Salonitis K, and Stournaras A. Nanomanufacturing processes: A critical review. Pro VRAP 2003; Portugal: 535-43.
- [97] Wozniak M, Graule T, Hazan Y, Kata D, and Lis J. Highly loaded UV curable nanosilica dispersions for rapid prototyping applications. J Euro Ceramic Soc 2009; 29 (11): 2259-65.
- [98] Gibson I, Savalani MM, Tarik A, and Liu Y. The use of multiple materials in Rapid Prototyping. Pro VRAP 2007; Portugal: 51-6.
- [99] Hong SB, Eliaz N, Sachs EM, Allen SM, and Latanision RM. Corrosion behaviour of advanced titanium-based alloys made by three-dimensional printing for bio-medical applications. Cor Sci 2001; 43(9) 1781-91.
- [100] Vandenbroucke B and Kruth JP. Selective laser melting of biocompatible metals for rapid manufacturing of medical parts. Rapid Proto J 2007; 13 (4) 196-203.
- [101] Van Bael S, Vandenbroucke B, Kerckhofs G, Schrooten J, and Kruth JP. Design and production of bone scaffolds with selective laser melting. Pro TMS 2009; San Francisco.
- [102] Partee B, Hollister SJ, and Das S. Selective laser sintering process optimization for layered manufacturing of CAPA(R) 6501 Polycapralactone bone tissue engineering scaffolds. J Manu Sci and Eng -Tran ASME 2006; 128 (2): 531-40.
- [103] Schmidt M, Pohle D, and Rechtenwald T. Selective Laser Sintering of PEEK. Ann CIRP; 56(1): 205-8.

- [104] Vandenbroucke B. Selective Laser Melting of Biocompatible parts for rapid manufacturing of medical parts. PhD thesis 2008, K. U. Leuven, Division PMA.
- [105] Kalita SJ, Bose S, Hosick HL, and Bandyopadhyay A. Development of controlled porosity polymer-ceramic composite scaffolds via fused deposition modeling. Mat Sci and Eng C 2003; 23: 611-20.
- [106] Chua CK, Leong KF, Tan KH, Wiria FE, and Cheah CM. Development of tissue scaffolds using selective laser sintering of polyvinyl alcohol/hydroxyapatite biocomposite for craniofacial and joint defects. J Mat Sci : Mat in Med 2004; 15 (10): 1113- 21.
- [107] Taboas JM, Maddox RD, Krebsbach PH, and Hollister SJ. Indirect solid free form fabrication of local and global porous, biomimetic and composite 3D polymer-ceramic scaffolds. Biomat 2003; 24: 181-94.
- [108] Yang S, Leong KF, Du Z, and Chua CK. The design of scaffolds for use in tissue engineering. part 2. rapid prototyping technique. Tissue Eng 2003; 8 (1): 1-11.
- [109] Leong KF, Chea CM, and Chua CK. Solid freeform fabrication of three-dimensional scaffolds for engineering replacement tissues and organs. Biomat 2003;24: 2363-78.
- [110] Cruz F, Coole T, Bocking C, and Simoes J. Selective laser sintering of customized medical implants using biocomposite materials. Tech Vjesn 2003; 10 (2): 23-7.
- [111] Chartoff R, Steidle C, Klosterman D, Graves G, and Osborne N. Automated fabrication of custom bone implants using rapid prototyping. Business Briefing: Medical Device Manu & Techno 2002; 1-4.
- [112] Gomes ME and Reis RL. Biodegradable polymers and composites in biomedical applications: from catgut to tissue engineering, part 2- systems for temporary replacement and advanced tissue regeneration. Int Mat Rev 2004; 49 (5): 274-85.
- [113] Gomes ME and Reis RL. Biodegradable polymers and composites in biomedical applications:from catgut to tissue engineering. part 1- available systems and their properties. Int Mat Rev 2004; 49 (5): 261-73.
- [114] Tan KH, Chua CK, Leong KF, Naing MW, and Cheah CM. Fabrication and characterization of three-dimensional poly(ether-ether-ketone)/-hydroxyapatite biocomposite scaffolds using laser sintering. Pro Ins Mech Eng Part H- J Eng Med 2004; 219(H3):183-94.
- [115] Wiria FE, Chua CK, Leong KF, et.al. Improved biocomposite development of poly(vinyl alcohol) and hydroxyapatite for tissue engineering scaffold fabrication using selective laser sintering. J Mat Sci -Mat Med 2008; 19 (3): 989-96.

- [116] Zhou WY, Lee SH, Wang M, et.al. Selective laser sintering of porous tissue engineering scaffolds from poly(L)/carbonated hydroxyapatite nanocomposite microspheres. J Mat Sci Mat Med 2008;19 (7): 2535-40.
- [117] Heo SJ, Kim SE, et. al. Fabrication and characterization of novel nano- and micro-HA/PCL composite scaffolds using a modified rapid prototyping process . J Biomedical Mat Res Part A 2009; 89A: 108-16.
- [118] Zheng Y, Hao L, Savalani MM, Harris RA, and Tanner KE. Characterization and dynamic mechanical analysis of selective laser sintered hydroxyapatite-filled polymeric composites. J Biomedical Mat Res Part A 2008; 86A (3): 607-16.
- [119] Savalani MM, Hao L, Zhang Y, et.al. Fabrication of porous biactive structures using the selective laser sintering technique. Pro Ins Mech Eng Part H J Eng Med 2007;221(H8): 873-86.
- [120] Hao L, Savalani MM, Zhang Y, et.al. Selective laser sintering of hydroxyapatite reinforced polyethylene composites for bioactive implants and tissue scaffold development. Pro ins mech eng Part L J Mat Des and App 2006; 220(H4): 521-31.
- [121] Cooke MN, Fisher JP, Dean D, Rimnac C, and Mikos AG. Use of Stereolithography to manufacture critical-sized 3D biodegradable scaffolds for bone ingrowth. J Biomedical Mat Res Part B App Biomat 2002; 64B:65-9.
- [122] Lee JW, Ahn G, Kim DS, and Cho DW. Development of nano- and microscale composite 3D scaffolds using PPF/DEF-HA and micro-stereolithography. Microelectro Eng 2009; 86 (4-6): 1465-67.
- [123] Sherwood JK, Riley SL, Palazzolo R, Brown SC, Monkhouse DC, M. Coates, L. G. Griffith, L. K. Landeen, and A. Ratcliffe. A three-dimensional osteochondral composite scaffold for articular cartilage repair. Biomat 2002; 23 (24):4739-51.
- [124] Murphy WL, Kohn DH, and Mooney DJ. Growth of continuous bonelike mineral within porous (lactide-co-glycolide) scaffolds in vitro. J Biomedical Mat Res 2000; 50 (1): 50-58.

Figure 1 Caption SEM micrographs of infiltrated WC-12Co

Sl. No.	Materials Used	Composites	References
1	Fe, graphite	MMC	[17]
2	Ti, graphite/diamond	MMC	[26]
3	Ti, SiC	MMC	[26]
4	AlSi, SiC	MMC	[26]
5	AlMg, SiC	MMC	[26]
6	Co, WC	MMC	[18]
7	Cu , Ni , Ti , B_4C	$\mathrm{Cu}/\mathrm{TiB}_2$	[27]
8	TiO_2 , Al, C	$\mathrm{TiC/Al_2O_3}$	[28]
9	SiC, PA	$\mathrm{SiC/PA}$	[29]
10	Cu, Ni, Ti, C	Cu/TiC	[27]
11	Polycarbonate, Graphite	PMC	[30]
12	Fe, SiC	MMC	[31]
13	ZrO_2 , Y_2O_3 , Al , Al_2O_3	CMC	[32]
14	acrylic-styrene, SiO_2	PMC	[33]

Table 1
Materials used for the direct fabrication of composites in SLS

Sl. No.	Main Materials Used	Composites	References
1	C, Ti-Cu alloy	TiC/Ti-Cu	[55]
2	WC, Co_3O_4	WC/Co	[54]
3	steel, bronze	steel/bronze	[57]

Table 2
Main Materials used for the fabrication of composites in 3DP

Sl. No.	Materials Used	Composites	References
1	Invar, TiC	MMC	[60]
2	Ti-6Al-4V, B	Ti-6Al-4V/TiB	[59]
3	Ti, TiC	$\mathrm{Ti}/\mathrm{TiC}\ \mathrm{FGM}$	[58]
4	Ti, TiB	MMC	[63]
5	$NiBSi, Cr_3C_2$	FGM	[64]
6	NiBSi, WC-Co	FGM	[64]
7	Ti-48Al-2Cr-2Nb, TiC	MMC	[65]
8	WC-Co	MMC	[66,67]

Table 3
Materials used for the direct fabrication of composites in LENS

Sl. No.	Materials Used	References
1	Carbon fibre, bisphenol A-epoxy,	
	hydroxycyclohexyl phenyl ketone, lauroyl peroxide	[74]
2	glass fibre, acrylic-based polymer	[72]
3	E-glass fibre, epoxy-based resin	[7]
4	E-glass fibre, acrylic-based resin	[7]
5	carbon fibre, acrylic-based resin	[7]
6	Aramid, acrylic-based resin	[7]

Table 4
Materials used for fabricating Fibre-reinforced composites (FRC) in SL

Sl. No.	Main Materials Used	Composites	References
1	Fe, Nylon	Fe/Nylon	[80]
2	Al, Alumina	Al/Alumina	[81]
3	ceramic, polymer	for piezoelectric	[82]

Table 5
Main Materials used for the fabrication of composites in FDM

LM Techniques	Sl. No.	Materials Used	References
SLS	1	Ni, Ti, Ca ₅ (PO ₄) ₃ OH	[37]
	2	PEEK, HA	[10,114]
	3	PVA, HA	[106,115]
	4	PLLA , HA	[110,116]
	5	PCL, HA	[9,117]
	6	PE, HA	[118]
	7	PA, HA	[119,118]
	8	HDPE, HA	[11,120]
LOM	1	Calcium phosphate glass, HA	[111]
SL	1	PPF, TCP	[121]
	2	PPF/DEF, HA	[122]
FDM	1	PP, TCP	[105]
	2	PCL, HA	[109]
3DP	1	PLGA, TCP	[123]

Table 6 Composites fabricated by various RP techniques for bio-medical applications